ETAB: A Benchmark Suite for Visual Representation Learning in Echocardiography

Ahmed M. Alaa UC Berkeley and UCSF Berkeley, CA amalaa@berkeley.edu Anthony Philippakis Broad Institute of MIT and Harvard Cambridge, MA

David Sontag MIT CSAIL and IMES Cambridge, MA dsontag@csail.mit.edu

Abstract

Echocardiography is one of the most commonly used diagnostic imaging modalities in cardiology. Application of deep learning models to echocardiograms can enable automated identification of cardiac structures, estimation of cardiac function, and prediction of clinical outcomes. However, a major hindrance to realizing the full potential of deep learning is the lack of large-scale, fully curated and annotated data sets required for supervised training. High-quality pre-trained representations that can transfer useful visual features of echocardiograms to downstream tasks can help adapt deep learning models to new setups using fewer examples. In this paper, we design a suite of benchmarks that can be used to pre-train and evaluate echocardiographic representations with respect to various clinically-relevant tasks using publicly accessible data sets. In addition, we develop a unified evaluation protocolwhich we call the echocardiographic task adaptation benchmark (ETAB)-that measures how well a visual representation of echocardiograms generalizes to common downstream tasks of interest. We use our benchmarking framework to evaluate state-of-the-art vision modeling pipelines. We envision that our standardized, publicly accessible benchmarks would encourage future research and expedite progress in applying deep learning to high-impact problems in cardiovascular medicine.

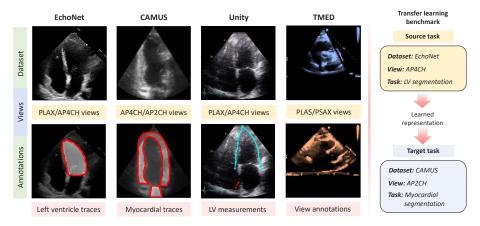


Figure 1: Visual task adaptation for echocardiography. Using multiple open- and public-access echocardiogram data sets, we develop a suite of benchmarks for representation and transfer learning in echocardiography.

36th Conference on Neural Information Processing Systems (NeurIPS 2022) Track on Datasets and Benchmarks.

1 Introduction and Motivation

Echocardiography is one of the most commonly used non-invasive imaging techniques for assessing cardiac function, examining heart anatomy and diagnosing cardiovascular diseases. An "echo" study is an ultrasound of the heart acquired by a cardiac sonographer through a transducer device—different acquisition angles by which the device is placed relative to the patient's heart provide different "views" of the heart anatomy. Echocardiograms inform cardiologists, surgeons, oncologists and emergency physicians on clinical decisions pertaining to treatment management and surgical planning [1–6]. Because of the central role it plays in cardiovascular medicine, there has been a significant interest in applying deep learning-based computer vision models to echocardiograms, with the ultimate goal of automating cardiac evaluation, reducing variance and improving reproducibility in interpreting echocardiograms, and predicting patient-specific clinical outcomes [7–14].

A key hindrance to wider engagement in research focusing on applying deep learning to echocardiography is the lack of large, standardized, publicly-accessible data sets with the annotations required for all downstream tasks of interest. This is because, in addition to the regulatory hurdles associated with publicly sharing clinical data, building such data sets is already a difficult task in itself—i.e., collecting all labels of interest would require examination of clinical reports, pre-selection of relevant echo views, and retrospective manual annotation by experts. Consequently, existing public data sets for echocardiography (e.g., [15-17]) tend to contain a modest number of samples, with only subsets of the annotations and views required for all possible downstream analyses.

Because many downstream tasks would share the same relevant echocardiographic features, access to high-quality representations of echocardiograms—i.e., representations that retain these features— could enable reusing the same pre-trained representations across many tasks rather than training a new model from scratch for each task [18–20], hence enabling adaptation of pre-trained models in setups where fewer annotated data might be available. We shall call such a procedure *visual task adaptation*— see Figure 1 for a pictorial illustration. Motivated by such thinking, this paper develops a standardized set of benchmark tasks for pre-training and/or evaluating visual models of echocardiography. Our goal is to increase engagement of researchers in a high-impact application domain by providing a systematic domain-specific benchmark through which researchers can focus their effort on tack-ling challenging problems peculiar to echocardiography, and translate methodological advances in representation learning to practical problems in cardiovascular medicine.

The contribution of this paper is two-fold. *First*, we develop a comprehensive suite of benchmark tasks tailored to echocardiography using a meta-dataset of public-access sources of echocardiographic data. These benchmark tasks can be used to test vision modeling pipelines, pre-train visual representations of echoes, and evaluate the transferability of representations across pairs of source-target tasks which might differ in the data source, echo views and annotations. *Second*, using our suite of benchmark tasks we specify a unified evaluation protocol for readily available pre-trained representations— the *echocardiographic task adaptation benchmark* (ETAB)—which is meant to evaluate the extent by which a given representation generalizes to different tasks, views and patient cohorts. The ETAB benchmark enables researchers to share a unified and publicly-accessible evaluation protocol, even when the representations themselves are pre-trained on private hospital data. ETAB is implemented as a full-fledged software package with a user-friendly API for researchers to design and evaluate visual representations for echocardiograms (Code available at: https://github.com/ahmedmalaa/ETAB).

2 Echocardiogram Datasets

The ETAB benchmark suite is based on 5 publicly accessible echocardiogram data sets that span different cohorts and involve different echocardiographic views and annotations (Table 1). In what follows, we provide a brief overview of all data sets currently supported in ETAB.

EchoNet. This data set has two variants: EchoNet-Dynamic and EchoNet-LVH. In the EchoNet-Dynamic data set, introduced in [15], one apical-4 chamber (AP4CH) 2D gray-scale video is extracted from each echo study. A total of 10,036 videos are collected from 10,036 distinct individuals who underwent echocardiography between 2006 and 2018 as part of routine care at a University Hospital. Individuals in the data set were selected at random from hospital records. Along with each video, cardiac function assessments and calculations obtained by a registered sonographer and verified by a level-3 echocardiographer are provided. The second data set, EchoNet-LVH, was collected for a

Data set	Sample size	Echo views	Annotations
EchoNet-Dynamic	10,036	AP4CH	LV traces and LV ejection fraction (EF)
EchoNet-LVH	12,000	PLAX	LV internal dimension, LV posterior wall, In- traventricular septum
Unity	1,224	AP4CH, PLAX	LV measurements and longitudinal strain
CAMUS	500	АР4СН, АР2СН	LV EF, ES/ED frames, LV epicardium, endo- cardium and left atrium segments
TMED	2,341	PLAX, PSAX, Other	Aortic Stenosis diagnoses, view annotations

similar cohort and comprises detailed measurements of the LV dimensions based on parasternal long axis (PLAX) views. Both data sets were released by Stanford AIMI Center and are accessible via: https://echonet.github.io/echoNet/ and https://echonet.github.io/lvh/.

Unity Imaging Collaborative. These echocardiograms were obtained from the British echocardiography laboratories and were retrospectively annotated by echocardiography-certified cardiologists through a UK-wide initiative that involved 17 hospitals [21]. The data set comprises a mixture of apical and parasternal views; the former is accompanied with measures of longitudinal strain, and the latter involves measures of LV dimensions. The data is accessible via: https://data.unityimaging.net/.

CAMUS. The Cardiac Acquisitions for Multi-structure Ultrasound Segmentation (CAMUS) is an open-access data set from 500 patients, acquired at the University Hospital of St. Etienne (France) [16]. Compared to EchoNet, this data set has a smaller sample size but is more elaborately annotated, hence it serves as an appropriate target data set for a variety of downstream tasks. The data set contains apical two- and four-chamber acquisitions (AP2CH and AP4CH). Half of the population has a left ventricle (LV) ejection fraction lower than 45%, thus being considered at pathological risk. The data set contains full annotation of the left atrium, the endocardium and epicardium borders of the LV, performed by a cardiologist. To identify the beginning and end of each cardiac cycle, ED and ES frames within each echo clip are labeled. Data is accessible via: https://www.creatis.insa-lyon.fr/Challenge/camus/.

TMED. The Tufts Medical Echocardiogram Dataset (TMED) contains still echocardiogram imagery acquired in the course of routine care from 2015 to 2020 [17]. This data set contains both labeled and unlabeled images—labels include a categorization of views into parasternal long and short axis views (PLAX and PSAX), and diagnostic severity ratings for aortic stenosis (AS). Unlike EchoNet, Unity and CAMUS, this data set contains only still images rather than sequences of frames. The data set is publicly available and can be accessed through: https://tmed.cs.tufts.edu/.

3 A Benchmark Suite for Echocardiographic Representation Learning

Our benchmark suite encapsulates a set of standardized tasks that cover a wide variety of echocardiographic modeling problems of interest. Each task comprises a selection of a data set, a view and an annotation from the options listed in Table 1. These standardized tasks can be used to benchmark the performance of vision models, pre-train visual representations, or evaluate the quality of externally pre-trained representations of echocardiograms. In Section 3.1, we present the ETAB benchmark tasks, and in Section 3.2 we describe our proposed ETAB evaluation protocol.

3.1 The ETAB benchmark tasks

Based on the data sets listed in Section 2, we design **31 benchmark tasks** that cover various echocardiographic tasks of interest. Each benchmark task comprises a specification of the data set, echo view and annotations. The benchmarks are divided into four categories: (•) cardiac structure identification (e.g., detecting the borders of the LV), (•) cardiac function estimation (e.g., estimating the LV ejection fraction), (•) view classification, and (•) clinical prediction. Benchmarks within the same category share a color code that will be later used in visualizations of experimental results. These benchmark tasks constitute the core of the ETAB evaluation protocol presented later in Section 3.2.

	Benchmark description					
	Benchmark code	Data set	View	Task		
re	• a0-A4-E	EchoNet-Dynamic	AP4CH	Left ventricle segmentation		
on tu	• a0-A4-C	CAMUS	AP4CH	Left ventricle segmentation		
ati	• a1-A4-C	CAMUS	AP4CH	Left atrium segmentation		
st fic	• a2-A4-C	CAMUS	AP4CH	Myocardial wall segmentation		
iac	• a0-A2-C	CAMUS	AP2CH	Left ventricle segmentation		
Cardiac structure identification	• a1-A2-C	CAMUS	AP2CH	Left atrium segmentation		
i	• a2-A2-C	CAMUS	AP2CH	Myocardial wall segmentation		
	• b0-A4-E	EchoNet-Dynamic	AP4CH	LV ejection fraction estimation		
	• b1-A4-E	EchoNet-Dynamic	AP4CH	Cardiac cycle phase estimation		
	• b2-PL-E	EchoNet-LVH	PLAX	Intraventricular septum estimation		
	• b3-PL-E	EchoNet-LVH	PLAX	LV internal dimension estimation		
ų	• b4-PL-E	EchoNet-LVH	PLAX	LV posterior wall identification		
Cardiac function estimation	• b0-A4-C	CAMUS	AP4CH	LV ejection fraction estimation		
cdiac funct estimation	• b0-A2-C	CAMUS	AP2CH	LV ejection fraction estimation		
: fu	• b1-A4-C	CAMUS	AP4CH	Cardiac cycle phase estimation		
itin	• b1-A2-C	CAMUS	AP2CH	Cardiac cycle phase estimation		
es r	• b5-A4-U	Unity	AP4CH	Identifying mitral hinge point on septum		
ũ	• b6-A4-U	Unity	AP4CH	Identifying mitral hinge point on lateral wall		
	• b7-A4-U	Unity	AP4CH	Identifying LV endocardial apex		
	• b8-A4-U	Unity	AP4CH	Identifying LV endocardial contour		
	• b2-PL-U	Unity	PLAX	Intraventricular septum estimation		
	• b3-PL-U	Unity	PLAX	LV internal dimension estimation		
	• b4-PL-U	Unity	PLAX	LV posterior wall identification		
uc						
N iii	• c1-XX-E	EchoNet		Classify AP4CH and PLAX views		
View recognition	• c0-XX-C	CAMUS		Classify AP4CH and AP2CH views		
∽ o	• c1-XX-U	Unity TMED		Classify AP4CH and PLAX views		
re	• с2-ХХ-Т	IMED		Classify PLAX and PSAX views		
Clinical prediction	• d0-A4-E	EchoNet-Dynamic	AP4CH	Diagnose cardiomyopathy		
nic.	d1-PL-T	TMED	PLAX	Diagnose Aortic Stenosis		
Clinical	• d0-A4-C	CAMUS	AP4CH	Diagnose cardiomyopathy		
Du	• d0-A2-C	CAMUS	AP2CH	Diagnose cardiomyopathy		

Table 2: List of all ETAB benchmark tasks. The tasks cover four categories: (•) cardiac structure identification, (•) cardiac function estimation, (•) view classification, and (•) clinical prediction. Each benchmark task is assigned a code that encodes a specification of the source data set, echocardiographic view and annotations.

Each benchmark is encoded through an 5-character code of the form XX-XX-X. The encoding scheme describes each benchmark in terms of the data source, echo view and modeling task follows:

- Characters 0-1: Task identifier
- Characters 2-3: View identifier
- Characters 4-5: Dataset identifier

The data sets are encoded as follows **E**: EchoNet, **C**: CAMUS, **U**: Unity, and **T**: TMED. The views are encoded as follows: **A2**: Apical 2-chamber, **A4**: Apical 4-chamber, **PL**: parasternal long axis, and **PS**: parasternal short axis. The 4 task categories are encoded as **a**, **b**, **c** and **d**, and the detailed list of codes for all tasks is provided in the Appendix. The task encoding provides a systematic way for running benchmark experiments and reporting results through the ETAB software library.

Transfer learning benchmarks. In addition to the core benchmark tasks listed in Table 2, benchmark setups for transfer learning can be constructed by picking pairs of source and target tasks from the ETAB task suite. The pairs of benchmark tasks would be typically selected so that at least one of the three elements of a task specification (i.e., data set, view or annotation) differs between the source and the target. These "adaptation" setups can be used to test the ability of a transfer learning algorithm

to repurpose pre-trained representations for new downstream tasks, and provide insights into which tasks and model architectures lead to the most generalizable representations of echocardiograms. A transfer learning benchmark is encoded as: **Source-task-code/Target-task-code**. For example, benchmark **a0-A4-E/b3-PL-U** involves pre-training a representation to segment the left ventricle using apical 4-chamber studies from EchoNet-Dynamic, and then using the resulting representation to estimate the LV internal dimension using PLAX studies from the unity data set.

Vision modeling pipelines. Each of the core benchmark tasks in Table 2 can be conducted using a *vision modeling pipeline* \mathcal{M} that comprises (1) a choice of a backbone architecture for the visual representation and a (2) task-specific model head as depicted in Figure 2. The backbone representation can either be pretrained using external data sources or trained from scratch on the benchmark task.

When applied to a transfer learning setup (i.e., a pair of source and target benchmark tasks from Table 2), the modeling pipeline retains the backbone representation trained on the source task and finetunes a task-specific head using data from the target task. This could help us answer questions such as: is LV segmentation a good pretext task for learning useful representations in patients with aortic stenosis? which architectures result in representations that generalize well across patient cohorts? How many echo studies do we need to annotate in order to finetune a pretrained model for a given downstream task? Answers to these questions can inform practical modeling choices and data collection requirements.

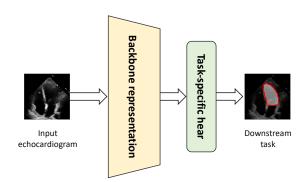


Figure 2: Depiction of a vision modeling pipeline \mathcal{M} .

3.2 The ETAB evaluation protocol

In many practical scenarios, we might be interested in evaluating how well a visual representation pretrained on an external data set captures echocardiographic features, e.g., private echocardiogram data, data for other cardiac imaging modalities, or even non-medical data sets (such as ImageNet). The echocardiographic task adaptation benchmark (ETAB) is a unified evaluation protocol that uses the core benchmark tasks in Table 2 to evaluate the usefulness of a given (pre-trained) visual representation for a wide variety of common downstream tasks in echocardiography.

Let $\mathcal{K} = \{1, \ldots, K\}$ be the benchmark categories, and let $\mathcal{T}_k = \{t_{1,k}, \ldots, t_{T_k,k}\}$ be the tasks within category $k \in \mathcal{K}$. (In Table 2, we have K = 4 task categories.) Let $\mathcal{D}_{t,k}$ be the data set associated with the *t*-th task within the *k*-th category. Let \mathcal{R}_{θ} be a pre-trained representation with an architectural specification \mathcal{R} and parameters θ . For each task t_k , we construct a model $\mathcal{M}_{\theta,\phi(t_k)} = \mathcal{R}_{\theta} \circ h_{\phi(t_k)}$, where $h_{\phi(t_k)}$ is a model head (e.g., a linear layer) that is specific to task t_k with parameters $\phi(t_k)$. For each task t_k , the corresponding data set $\mathcal{D}_{t,k}^n = \{(X_{t,k}^i, Y_{t,k}^i)\}_{i=1}^n$ is used to optimize the parameters of the task-specific head ϕ^* , with the representation parameters θ fixed. Let $\mathcal{E}_{t,k}$ be the evaluation metric used to assess performance on task t_k , which we assume takes on values in [0, 1]. The ETAB score of a pre-trained representation \mathcal{R}_{θ} is thus defined as:

$$\operatorname{ETAB}_{k}^{n}(\mathcal{R}_{\theta}) \triangleq \mathbb{E}_{t \sim P_{\mathcal{T}_{k}}} \mathcal{E}_{t,k} \left[\mathcal{M}_{\theta,\phi^{*}(t_{k})}(\mathcal{D}_{t,k}^{n}) \right], \ \operatorname{ETAB}^{n}(\mathcal{R}_{\theta}) \triangleq \mathbb{E}_{k \sim P_{\mathcal{K}}} \operatorname{ETAB}_{k}^{n}(\mathcal{R}_{\theta}).$$
(1)

The ETAB score can be evaluated for different values of n to assess the sample efficiency, i.e., transferability, of a pre-trained representation. We implement the metric in (1) by assigning equal weights to all benchmark tasks across all task categories, i.e., $P_{\mathcal{T}_k}$ and $P_{\mathcal{K}}$ are uniform distributions. A weighted ETAB score (with non-uniform choice of $P_{\mathcal{T}_k}$ and $P_{\mathcal{K}}$) can be defined to reflect the relative importance or frequency of the different echocardiographic tasks in Table 2 in real-world settings.

The ETAB protocol is model-agnostic, hence it can serve as a benchmark against which all existing and future architectural choices \mathcal{R} and pre-training algorithms can be evaluated. This includes representations pre-trained using supervised, semi-supervised, self-supervised, and generative approaches. Unlike the individual benchmark tasks in Section 3.1—which assess specific downstream or transfer learning scenarios—the ETAB protocol assesses the general usefulness of a visual representation to

echocardiographic tasks through a single procedure and metric. Currently, the total number of benchmark tasks involved in ETAB is 31. We envision that the number of ETAB tasks will grow as more data sets and annotations for echocardiograms are released for public access over time.

To the best of our knowledge, ETAB is the first systematic benchmarking setup dedicated to evaluating echocardiographic representations. Our benchmarking setup can be considered as the domain-specific analogue of the general benchmark for vision tasks developed in [19, 20]. (Further discussion on related work is provided in the supplement.) Models that perform well on general benchmarks may not necessarily be as competitive on downstream tasks specific to echo data, which creates the need for benchmarks that are tailored to the tasks most relevant to cardiovascular problems. A schematic depiction of the protocol is provided in Figure 3.

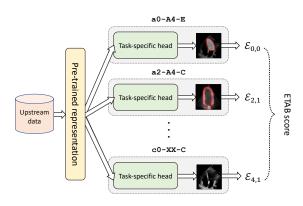


Figure 3: Schematic depiction of the ETAB protocol.

4 The ETAB Software Library

The ETAB library is a PyTorch-based implementation of our benchmarking framework that provides a unified and easy-to-use API for running benchmark experiments out-of-the-box, developing new vision modeling pipelines for echocardiography and evaluating pre-trained representations using the ETAB score. The ETAB library offers two key features:

- A unified API for loading and processing publicly-accessible echocardiography datasets.
- An easy-to-use API for creating modeling pipelines that supports a wide variety of backbone architectures and covers the benchmark tasks in Table 2.

The ETAB package can be installed via https://github.com/ahmedmalaa/ETAB. In this Section, we describe the key features of the package along with representative results for benchmark experiments.

4.1 Key features and examples of usage

ETAB data sets. The ETAB library supports a unified API for all public-access data sets listed in Table 1. The ETAB_dataset class is a container for echocardiography data with a multitude of options that specify the data source, echo view, annotations and parameters of the echo study clip (e.g., resolution and frame size, clip length, frame sampling rates). An example for instantiating a data set of apical 4-chamber echo studies with LV EF measurements is provided below:

```
import etab
```

The ETAB_dataset comes with built-in functionalities for loading and processing the data. A detailed description of these functionalities can be found in the ETAB package documentation.

ETAB model zoo. The ETAB package supports a variety of built-in vision modeling pipelines. Currently, the package supports **12** backbone representations that belong to the convolutional neural network (CNN) and vision transformer (ViT) families. Note that some benchmark tasks (e.g., estimation of LV ejection fraction) are defined with respect to video clips rather than still images, whereas other tasks and datasets are limited to 2D images. In the current release of ETAB, we restrict the backbone representations to frame embeddings and use these representations repeatedly over sequences of images. By restricting the backbone representations to frame embeddings, we ensure that the backbone architecture can be used systematically across all benchmark tasks. In Section 4.3,

we describe the task-specific heads for all benchmark categories in Table 2. The ETAB model zoo (all of the supported backbone and model heads) is available in the Supplementary material.

ETAB score computation. To compute the ETAB score for a given pre-trained representation, the user can load the pre-trained weights for a PyTorch implementation of any of the supported backbones, and then invoke the ETABscore function to evaluate the quality of the representation as follows:

In the example above, we load a ResNet-50 model pre-trained on the ImageNet-1K data set and then evaluate its ETAB score, i.e., measure how well a ResNet-50 trained on non-medical imaging data captures echocardiographic features. By default, the ETAB score is evaluated assuming a uniform weight for all benchmark tasks and with the pre-trained weights being frozen across all tasks. The ETABscore function also supports full finetuning and weighted sampling of benchmark tasks.

Evaluation metrics. We use the following evaluation metrics within the ETAB evaluation protocol in Equation (1). For all segmentation tasks, the metric $\mathcal{E}_{t,k}$ corresponds to the DICE score. For classification tasks, $\mathcal{E}_{t,k}$ is defined as the area under the ROC curve (AUC-ROC). For regression tasks (i.e., predicting LV EF), we use R^2 as the metric $\mathcal{E}_{t,k}$. All metrics are computed on held-out samples. Note that, while we use different metrics for the different tasks, all metrics are defined in the normalized range [0, 1] (higher is better). To compute the ETAB score for a given baseline, we run all benchmark tasks in Table 2 and average the resulting evaluation metrics.

4.2 ETAB modeling pipelines

As discussed in the previous Section, ETAB supports backbone representations \mathcal{R}_{θ} that belong to the CNN and ViT architectural families. The CNN backbones include: ResNet [22], ResNeXt [23], DenseNet [24], Inception [25], MobileNet [26] and ConvNext [27]. The ViT backbones include: Mix Transformer encoders (MiT) [28], Pyramid Vision Transformer (PVT) [29], Multi-scale vision Transformer (ResT) [30], PoolFormer [31], and UniFormer [32]. In what follows, we describe the task-specific heads h_{ϕ} for the four benchmark categories in Table 2.

(•) Task-specific heads for cardiac structure identification benchmarks.

The "cardiac structure identification" tasks (•) involve semantic segmentation of ventricular and other anatomic structures. We consider the following segmentation heads: U-Net [33], U-Net++ [34], MAnet [35], Linknet [36], PSPNet [37], DeepLabV3 [38], TopFormer and SegFormer [28]. Depending on the architecture of the selected backbone representation, the default segmentation head used in the ETABscore function is either a U-Net or a SegFormer.

(•) *Task-specific heads for cardiac function estimation benchmarks.*

This category of tasks involve estimating a patient's cardiac output from an echocardiography video. For all tasks in this category, we apply the backbone representations to obtain frame-level embeddings for the sequence of frames in each echo study. The task-specific heads are variants of recurrent neural networks (RNN) applied to these frame embeddings to obtain a representation for the sequence.

(•, •) Task-specific heads for view classification and clinical predictions.

For all benchmark tasks in this category, we considered baseline models that train attach a simple linear layer on top of the backbone representation to evaluate the output prediction.

The ETABmodel class in ETAB provides a unified sklearn-like API for all vision modeling pipelines. Examples of usage of the ETAB modeling pipelines are provided in the demo notebooks within the ETAB package documentation. Evaluations of the ETAB scores for state-of-the-art backbone models are maintained and regularly updated on the online ETAB leaderboard. In the rest of this Section, we provide sample results for applying the vision modeling pipelines to the benchmark tasks in Table 2.

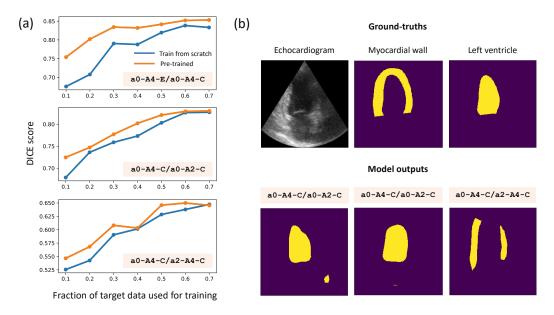


Figure 4: **Results for the cardiac structure identification benchmarks** (•). (a) Performance of the SegFormer model head with a ResNet-50 backbone with and without pre-training on the source data in each transfer learning benchmark. (b) Ground-truth traces (top) and samples of the recovered segmentation by the model (bottom).

4.3 Transfer learning benchmarks

In this Section, we consider the **cardiac structure identification benchmarks** (•) in Table 2. Here , the goal is to segment various anatomic structures of relevance to cardiac diagnostics. In particular, the tasks cover segmentation of the left ventricle (LV), the left atrium (LA), and myocardial wall (MY). LV segmentation is used to compute cardiac contractile function parameters (e.g., systolic/diastolic volumes, ejection fraction, and myocardium mass), which are key indicators of cardiac health [39]. Similarly, segmental evaluation of the MY and LA confer diagnostic value since MY wall thickness and LA enlargement are associated with pathological conditions such as hypertrophy [40].

Based on these benchmarks, we consider 3 experimental setups designed to test the transferability of features across data sets, echo views and tasks. Setup a0-A4-C/a0-A2-C can be used to assess the transferability of ML models across 4- and 2-chamber views, setups a0-A4-C/a1-A4-C and a0-A4-C/a2-A4-C assesses transferability across targets, whereas a0-A4-E/a0-A4-C tests transferability across data sets. Setups a0-A4-E/a0-A2-C and a0-A4-E/a2-A2-C are more challenging as they involve changing data sets, views and labels between the source and target tasks.

In Figure 4 (a), we show the performance of the SegFormer head with a ResNet-50 backbone for setups **a0-A4-E/a0-A4-C**, **a0-A4-C/a0-A2-C** and **a0-A4-C/a2-A4-C**. We evaluate the sample efficiency of the baseline model by fixing the number of training examples in the source task, and varying the number of training examples within the target task. This setup emulates the real-world scenario where we would have few echocardiographic studies extracted from hospital records for a cohort of interest that are manually annotated by a cardiologist, and we would like to adapt a model pre-trained on data from a different hospital to the cohort under study. Stronger baselines would enable us to collect and manually annotate less data points.

The results in Figure 4 (a) demonstrate the relative difficulty of the different transfer learning tasks in terms of the number of (target) examples required for competitive performance. For each of the benchmark tasks, we compare an adaptation pipeline that pre-trains the model on the source task with training from scratch on the target task. For the a0-A4-E/a0-A4-C and a0-A4-C/a0-A2-C setups, we observe that pre-training on source task significantly outperforms supervised learning from scratch when the number of target samples is as few as 16 target examples. From a practical perspective, this means that we can use these benchmarks to select adaptation pipelines for small-scale studies involving echocardiography data (e.g., clinical trial data), and expect the selected model to per-

	Benchmark	U-Net	U-Net++	MAnet	Linknet	PSPNet	DeepLabV3
н. Н	• a0-A4-C/a0-A2-C	0.885	0.893	0.752	0.892	0.847	0.840
10 10	• a0-A4-C/a1-A4-C	0.729	0.705	0.739	0.481	0.684	0.659
stı cat	• a0-A4-C/a2-A4-C	0.540	0.494	0.539	0.709	0.532	0.666
ifi	• a0-A4-E/a0-A4-C	0.909	0.804	0.898	0.896	0.900	0.909
ent Ent	• a0-A4-E/a0-A2-C	0.891	0.774	0.882	0.894	0.883	0.879
Cardiac struct. identification	• a0-A4-E/a2-A4-C	0.634	0.603	0.691	0.580	0.707	0.671

Table 3: **Performance of different segmentation heads on cardiac structure identification benchmarks.** In all experiments, we use 32 training examples in the target task. All baselines use ResNet-50 backbone as the encoder architecture. Reported numbers are DICE scores on a test set; bold values correspond to best performing baseline.

form competitively on the data set at hand even if the number of samples is small. Samples of the boundaries of LV and MY detected by the adapted models are illustrated in Figure 4 (b).

Figure 4 (a) shows that, while transfering learned features across data sets and across echo views is feasible, transferring representations across different labels (i.e., LV and MY) is a difficult task. We observe that for setup a0-A4-C/a2-A4-C, pre-training on the source task was no better than training from scratch on target data. The difficulty of this benchmark task inspires future research that focuses on developing adaptation pipelines that use other approaches, such as self-supervised or multi-task learning, to improve the transferability of features across the LV and MY labels.

Table 3 demonstrates the performance of all segmentation heads with the ResNet-50 backbone on 6 transfer learning benchmarks. We observe that no modeling pipeline uniformly outperforms others on all benchmarks, which suggests that our benchmark suite can be used for model selection in new downstream tasks. Overall, we found that transfer learning benchmarks involving label shift (e.g., a0-A4-C/a1-A4-C and a0-A4-C/a2-A4-C) are more difficult than benchmarks involving shift in data sets or views. Benchmarks that involved label shifts also exhibited larger variance in the observed performance of the different modeling baselines.

Representation	Weights	ETAB score	Representation	Weights	ETAB score
MobileNet-V2	ImageNet-1K	0.783	PoolFormer-S24	ImageNet-1K	0.692
ResNet-50	Fully finetuned	0.769	MiT-B2	Fully finetuned	0.691
MobileNet-V3-Large	Fully finetuned	0.749	ResNet-50	ImageNet-1K	0.689
ResNet-18	ImageNet-1K	0.702	MiT-B2	ImageNet-1K	0.653
ResNet-34	ImageNet-1K	0.699	ConvNext-Base	Fully finetuned	0.647

Table 4: ETAB scores for various backbone representations.

4.4 Evaluating pre-trained representations using the ETAB protocol

Finally, we compare various pre-trained backbone representations with respect to their ETAB scores and report the results in Table 4. Here, we evaluate the ETAB scores by tuning the different backbone models to tasks **a0-A4-E**, **a0-A4-C**, **a0-A2-C**, **a1-A4-C**, and **a1-A2-C**, with equal weights for all tasks. We explore two variants of each backbone model: freezing the pre-trained ImageNet-1K weights and tuning the head, and fully finetuning the entire model for each benchmark task. The backbone models included CNN architectures (ResNet, MobileNet, ConvNext), as well ViT models (MiT and PoolFormer). Table 4 lists the ETAB scores for all backbone models. A visualization for the break down of the task-specific ETAB scores is available in the online leaderboard.

Overall, we found that the CNN-variants outperformed their ViT counterparts. Moreover, full finetuning on the ETAB data sets did not significantly improve the ETAB scores for most backbone models. An interesting use case for our the ETAB framework is to explore whether pre-training backbone representations on large-scale medical imaging data sets, such as RadImageNet [41], could outperform the ImageNet-pretrained backbone with respect to the ETAB score.

5 Conclusion

Deep learning can help automate the echocardiography workflow and refine our understanding of heart disease subtypes using cardiac ultrasound data. The scarcity and sporadicity of publicly accessible echocardiogram data sets create a need for standardized benchmarks in order to encourage engagement in research applying state-of-the-art representation learning methods to echocardiographic data. This paper takes a first step towards building a standardized framework for benchmarking the quality of representations for echocardiograms. We hope that the benchmark tasks and evaluation methods presented in this paper will lower the barrier to translating advances in visual representation learning into impactful applications in the medical domain.

Acknowledgments and Disclosure of Funding

Funding to support this research was provided for by the Eric and Wendy Schmidt Center at the Broad Institute of MIT and Harvard (https://www.broadinstitute.org/ewsc.).

References

- [1] Robert R Moss, Emma Ivens, Sanjeevan Pasupati, Karin Humphries, Christopher R Thompson, Brad Munt, Ajay Sinhal, and John G Webb. Role of echocardiography in percutaneous aortic valve implantation. *JACC: Cardiovascular Imaging*, 1(1):15–24, 2008.
- [2] G Habib and A Torbicki. The role of echocardiography in the diagnosis and management of patients with pulmonary hypertension. *European Respiratory Review*, 19(118):288–299, 2010.
- [3] Jennifer Liu, Jose Banchs, Negareh Mousavi, Juan Carlos Plana, Marielle Scherrer-Crosbie, Paaladinesh Thavendiranathan, and Ana Barac. Contemporary role of echocardiography for clinical decision making in patients during and after cancer therapy. *JACC: Cardiovascular Imaging*, 11(8):1122–1131, 2018.
- [4] Guy R Randolph, Donald J Hagler, Heidi M Connolly, Joseph A Dearani, Francisco J Puga, Gordon K Danielson, Martin D Abel, V Shane Pankratz, and Patrick W O'Leary. Intraoperative transesophageal echocardiography during surgery for congenital heart defects. *The Journal of Thoracic and Cardiovascular Surgery*, 124(6):1176–1182, 2002.
- [5] Meredith K Ford, W Scott Beattie, and Duminda N Wijeysundera. Systematic review: prediction of perioperative cardiac complications and mortality by the revised cardiac risk index. *Annals of internal medicine*, 152(1):26–35, 2010.
- [6] Raphael Rosenhek, Ursula Klaar, Michael Schemper, Christine Scholten, Maria Heger, Harald Gabriel, Thomas Binder, Gerald Maurer, and Helmut Baumgartner. Mild and moderate aortic stenosis: natural history and risk stratification by echocardiography. *European Heart Journal*, 25(3):199–205, 2004.
- [7] David Ouyang, Bryan He, Amirata Ghorbani, Neal Yuan, Joseph Ebinger, Curtis P Langlotz, Paul A Heidenreich, Robert A Harrington, David H Liang, Euan A Ashley, et al. Video-based ai for beat-to-beat assessment of cardiac function. *Nature*, 580(7802):252–256, 2020.
- [8] Grant Duffy, Paul P Cheng, Neal Yuan, Bryan He, Alan C Kwan, Matthew J Shun-Shin, Kevin M Alexander, Joseph Ebinger, Matthew P Lungren, Florian Rader, et al. High-throughput precision phenotyping of left ventricular hypertrophy with cardiovascular deep learning. *JAMA cardiology*, 7(4):386–395, 2022.
- [9] KY Esther Leung and Johan G Bosch. Automated border detection in three-dimensional echocardiography: principles and promises. *European journal of echocardiography*, 11(2):97–108, 2010.
- [10] Sumeet Gandhi, Wassim Mosleh, Joshua Shen, and Chi-Ming Chow. Automation, machine learning, and artificial intelligence in echocardiography: a brave new world. *Echocardiography*, 35(9):1402–1418, 2018.
- [11] Sukrit Narula, Khader Shameer, Alaa Mabrouk Salem Omar, Joel T Dudley, and Partho P Sengupta. Machine-learning algorithms to automate morphological and functional assessments in 2d echocardiography. *Journal of the American College of Cardiology*, 68(21):2287–2295, 2016.

- [12] Manar D Samad, Alvaro Ulloa, Gregory J Wehner, Linyuan Jing, Dustin Hartzel, Christopher W Good, Brent A Williams, Christopher M Haggerty, and Brandon K Fornwalt. Predicting survival from large echocardiography and electronic health record datasets: optimization with machine learning. *JACC: Cardiovascular Imaging*, 12(4):681–689, 2019.
- [13] Kenya Kusunose, Akihiro Haga, Takashi Abe, and Masataka Sata. Utilization of artificial intelligence in echocardiography. *Circulation Journal*, pages CJ–19, 2019.
- [14] Federico M Asch, Theodore Abraham, Madeline Jankowski, Jayne Cleve, Mike Adams, Nathanael Romano, Nicolas Polivert, Ha Hong, and Roberto Lang. Accuracy and reproducibility of a novel artificial intelligence deep learning-based algorithm for automated calculation of ejection fraction in echocardiography. *Journal of the American College of Cardiology*, 73(9S1):1447–1447, 2019.
- [15] David Ouyang, Bryan He, Amirata Ghorbani, Matt P Lungren, Euan A Ashley, David H Liang, and James Y Zou. Echonet-dynamic: a large new cardiac motion video data resource for medical machine learning. In *NeurIPS ML4H Workshop: Vancouver, BC, Canada*, 2019.
- [16] Sarah Leclerc, Erik Smistad, Joao Pedrosa, Andreas Østvik, Frederic Cervenansky, Florian Espinosa, Torvald Espeland, Erik Andreas Rye Berg, Pierre-Marc Jodoin, Thomas Grenier, et al. Deep learning for segmentation using an open large-scale dataset in 2d echocardiography. *IEEE* transactions on medical imaging, 38(9):2198–2210, 2019.
- [17] Zhe Huang, Gary Long, Benjamin Wessler, and Michael C Hughes. A new semi-supervised learning benchmark for classifying view and diagnosing aortic stenosis from echocardiograms. In *Machine Learning for Healthcare Conference*, pages 614–647. PMLR, 2021.
- [18] Fuzhen Zhuang, Zhiyuan Qi, Keyu Duan, Dongbo Xi, Yongchun Zhu, Hengshu Zhu, Hui Xiong, and Qing He. A comprehensive survey on transfer learning. *Proceedings of the IEEE*, 109(1):43–76, 2020.
- [19] Xiaohua Zhai, Joan Puigcerver, Alexander Kolesnikov, Pierre Ruyssen, Carlos Riquelme, Mario Lucic, Josip Djolonga, Andre Susano Pinto, Maxim Neumann, Alexey Dosovitskiy, et al. The visual task adaptation benchmark. 2019.
- [20] Xiaohua Zhai, Joan Puigcerver, Alexander Kolesnikov, Pierre Ruyssen, Carlos Riquelme, Mario Lucic, Josip Djolonga, Andre Susano Pinto, Maxim Neumann, Alexey Dosovitskiy, et al. A large-scale study of representation learning with the visual task adaptation benchmark. arXiv preprint arXiv:1910.04867, 2019.
- [21] James P Howard, Catherine C Stowell, Graham D Cole, Kajaluxy Ananthan, Camelia D Demetrescu, Keith Pearce, Ronak Rajani, Jobanpreet Sehmi, Kavitha Vimalesvaran, G Sunthar Kanaganayagam, et al. Automated left ventricular dimension assessment using artificial intelligence developed and validated by a uk-wide collaborative. *Circulation: Cardiovascular Imaging*, 14(5):e011951, 2021.
- [22] Kaiming He, Xiangyu Zhang, Shaoqing Ren, and Jian Sun. Deep residual learning for image recognition. In *Proceedings of the IEEE conference on computer vision and pattern recognition*, pages 770–778, 2016.
- [23] Saining Xie, Ross Girshick, Piotr Dollár, Zhuowen Tu, and Kaiming He. Aggregated residual transformations for deep neural networks. In *Proceedings of the IEEE conference on computer vision and pattern recognition*, pages 1492–1500, 2017.
- [24] Forrest Iandola, Matt Moskewicz, Sergey Karayev, Ross Girshick, Trevor Darrell, and Kurt Keutzer. Densenet: Implementing efficient convnet descriptor pyramids. *arXiv preprint arXiv:1404.1869*, 2014.
- [25] Christian Szegedy, Vincent Vanhoucke, Sergey Ioffe, Jon Shlens, and Zbigniew Wojna. Rethinking the inception architecture for computer vision. In *Proceedings of the IEEE conference* on computer vision and pattern recognition, pages 2818–2826, 2016.
- [26] Andrew Howard, Mark Sandler, Grace Chu, Liang-Chieh Chen, Bo Chen, Mingxing Tan, Weijun Wang, Yukun Zhu, Ruoming Pang, Vijay Vasudevan, et al. Searching for mobilenetv3. In *Proceedings of the IEEE/CVF international conference on computer vision*, pages 1314–1324, 2019.
- [27] Zhuang Liu, Hanzi Mao, Chao-Yuan Wu, Christoph Feichtenhofer, Trevor Darrell, and Saining Xie. A convnet for the 2020s. *arXiv preprint arXiv:2201.03545*, 2022.

- [28] Enze Xie, Wenhai Wang, Zhiding Yu, Anima Anandkumar, Jose M Alvarez, and Ping Luo. Segformer: Simple and efficient design for semantic segmentation with transformers. Advances in Neural Information Processing Systems, 34, 2021.
- [29] Wenhai Wang, Enze Xie, Xiang Li, Deng-Ping Fan, Kaitao Song, Ding Liang, Tong Lu, Ping Luo, and Ling Shao. Pvt v2: Improved baselines with pyramid vision transformer. *Computational Visual Media*, 8(3):415–424, 2022.
- [30] Qinglong Zhang and Yu-Bin Yang. Rest: An efficient transformer for visual recognition. *Advances in Neural Information Processing Systems*, 34:15475–15485, 2021.
- [31] Weihao Yu, Mi Luo, Pan Zhou, Chenyang Si, Yichen Zhou, Xinchao Wang, Jiashi Feng, and Shuicheng Yan. Metaformer is actually what you need for vision. In *Proceedings of the IEEE/CVF Conference on Computer Vision and Pattern Recognition*, pages 10819–10829, 2022.
- [32] Kunchang Li, Yali Wang, Junhao Zhang, Peng Gao, Guanglu Song, Yu Liu, Hongsheng Li, and Yu Qiao. Uniformer: Unifying convolution and self-attention for visual recognition. *arXiv* preprint arXiv:2201.09450, 2022.
- [33] Olaf Ronneberger, Philipp Fischer, and Thomas Brox. U-net: Convolutional networks for biomedical image segmentation. In *International Conference on Medical image computing and computer-assisted intervention*, pages 234–241. Springer, 2015.
- [34] Zongwei Zhou, Md Mahfuzur Rahman Siddiquee, Nima Tajbakhsh, and Jianming Liang. Unet++: A nested u-net architecture for medical image segmentation. In *Deep learning in medical image analysis and multimodal learning for clinical decision support*, pages 3–11. Springer, 2018.
- [35] Tongle Fan, Guanglei Wang, Yan Li, and Hongrui Wang. Ma-net: A multi-scale attention network for liver and tumor segmentation. *IEEE Access*, 8:179656–179665, 2020.
- [36] Abhishek Chaurasia and Eugenio Culurciello. Linknet: Exploiting encoder representations for efficient semantic segmentation. In 2017 IEEE Visual Communications and Image Processing (VCIP), pages 1–4. IEEE, 2017.
- [37] Hengshuang Zhao, Jianping Shi, Xiaojuan Qi, Xiaogang Wang, and Jiaya Jia. Pyramid scene parsing network. In *Proceedings of the IEEE conference on computer vision and pattern* recognition, pages 2881–2890, 2017.
- [38] Liang-Chieh Chen, George Papandreou, Florian Schroff, and Hartwig Adam. Rethinking atrous convolution for semantic image segmentation. *arXiv preprint arXiv:1706.05587*, 2017.
- [39] Shusil Dangi, Ziv Yaniv, and Cristian A Linte. Left ventricle segmentation and quantification from cardiac cine mr images via multi-task learning. In *International Workshop on Statistical Atlases and Computational Models of the Heart*, pages 21–31. Springer, 2018.
- [40] Phong T Lee, Marc R Dweck, Sparsh Prasher, Anoop Shah, Steve E Humphries, Dudley J Pennell, Hugh E Montgomery, and John R Payne. Left ventricular wall thickness and the presence of asymmetric hypertrophy in healthy young army recruits: data from the large heart study. *Circulation: Cardiovascular Imaging*, 6(2):262–267, 2013.
- [41] Xueyan Mei, Zelong Liu, Philip M Robson, Brett Marinelli, Mingqian Huang, Amish Doshi, Adam Jacobi, Chendi Cao, Katherine E Link, Thomas Yang, et al. Radimagenet: An open radiologic deep learning research dataset for effective transfer learning. *Radiology: Artificial Intelligence*, 4(5):e210315, 2022.
- [42] Yuanwei Li, Chin Pang Ho, Matthieu Toulemonde, Navtej Chahal, Roxy Senior, and Meng-Xing Tang. Fully automatic myocardial segmentation of contrast echocardiography sequence using random forests guided by shape model. *IEEE transactions on medical imaging*, 37(5):1081– 1091, 2017.
- [43] Mohammad H Jafari, Hany Girgis, Zhibin Liao, Delaram Behnami, Amir Abdi, Hooman Vaseli, Christina Luong, Robert Rohling, Ken Gin, Terasa Tsang, et al. A unified framework integrating recurrent fully-convolutional networks and optical flow for segmentation of the left ventricle in echocardiography data. In *Deep learning in medical image analysis and multimodal learning* for clinical decision support, pages 29–37. Springer, 2018.

- [44] Ming Li, Chengjia Wang, Heye Zhang, and Guang Yang. Mv-ran: Multiview recurrent aggregation network for echocardiographic sequences segmentation and full cardiac cycle analysis. *Computers in biology and medicine*, 120:103728, 2020.
- [45] Xin Liu, Yiting Fan, Shuang Li, Meixiang Chen, Ming Li, William Kongto Hau, Heye Zhang, Lin Xu, and Alex Pui-Wai Lee. Deep learning-based automated left ventricular ejection fraction assessment using 2-d echocardiography. *American Journal of Physiology-Heart and Circulatory Physiology*, 321(2):H390–H399, 2021.
- [46] Ali Madani, Ramy Arnaout, Mohammad Mofrad, and Rima Arnaout. Fast and accurate view classification of echocardiograms using deep learning. *NPJ digital medicine*, 1(1):1–8, 2018.
- [47] Sylvestre-Alvise Rebuffi, Hakan Bilen, and Andrea Vedaldi. Learning multiple visual domains with residual adapters. *Advances in neural information processing systems*, 30, 2017.
- [48] Eleni Triantafillou, Tyler Zhu, Vincent Dumoulin, Pascal Lamblin, Utku Evci, Kelvin Xu, Ross Goroshin, Carles Gelada, Kevin Swersky, Pierre-Antoine Manzagol, et al. Meta-dataset: A dataset of datasets for learning to learn from few examples. arXiv preprint arXiv:1903.03096, 2019.
- [49] Mingyu Ding, Bin Xiao, Noel Codella, Ping Luo, Jingdong Wang, and Lu Yuan. Davit: Dual attention vision transformers. *arXiv preprint arXiv:2204.03645*, 2022.

Supplementary Material

Statement on ethical implications. The ETAB framework provides a standardized API for loading and processing all datasets for the sake of model development and training, but it does not alter, distribute or directly share the datasets. Please make sure to follow the terms of the respective Research Use Agreements for all datasets upon access. Links to the data licenses for all datasets are available in the ETAB documentation. Please note that the ETAB library is **not meant to be used within clinical workflows**. Please use ETAB for research and model derivation purposes. Please also note that any sources of bias inherent in the datasets covered by ETAB might be reflected in the derived modeling pipelines and the corresponding ETAB scores.

Computing resources. All experiments in this paper were conducted using computational resources on Google Cloud Platform (GCP). Each individual benchmark experiment was conducted using an NVIDIA A100 GPU on a GCP virtual machine.

Dataset details. Table S1 provides an overview of the features and characteristics of all datasets currently incorporated into the ETAB benchmarking framework.

	EchoNet	CAMUS	TMED
Sample size	10,036	500	2,341
Echo views	AP4CH	AP4CH, AP2CH	PLAX, PSAX and other
Annotations	LV traces and LVEF	LVEF, ES/ED frames, LV epi-, endo-cardium and LA segments	AS diagnoses, view labels
Labeled data	All studies	All studies	260 studies
Frame sizes	112x112 pixels	Variable per study	64x64 pixels
Video clips	Available	Available	Unavailable

Table S1: Details of all echocardiographic datasets in ETAB.

A Related work

Deep Learning for echocardiography. Previous work on applying deep learning models to echocardiography has focused on automating the echo pipeline, i.e., training a model to conduct the cardiac measurements and traces that would otherwise be normally performed manually by clinicians. Previous work on the first category of tasks (• Cardiac structure identification) developed various approaches for segmenting cardiac structures based on single frames or sequences of frames in an echo clip. Existing models have either relied on completely data-driven approaches [34, 39] or a combination of deep learning modeling and statistical shape models [42]. Deep learning models for segmenting the left ventricle and the myocardial shape included U-Nets, LSTMs and 3D CNNs and DeepLabV3 [7, 43, 44]. Our benchmarking framework allows testing these different methodologies in a systematic fashion. The different data structures in the EchoNet, CAMUS and TMED data sets allow benchmarking the tasks of LV and myocardial segmentation using both static and temporal data. Previous work on (• Cardiac function estimation) developed models for predicting LVEF on the basis of both 2D images or 3D video frames using 3DCNNs or recurrent neural network architectures (RNN) [7, 14, 45]. Our benchmarks cover both setups; it can enable evaluating LV segmentation based on 2D images by replacing the LSTM prediction head with a repeatedly applied feedforward neural network. Our benchmarking framework can also be used to evaluate the adaptability of existing models for (• view recognition), e.g., [46], on new views (different from the ones originally involved in model training) as our benchmarks include apical 2- and 4-chamber views along with the parasternal views.

Benchmarks for computer vision models. To the best of our knowledge, ETAB is the first systematic benchmarking setup dedicated to evaluating echocardiographic representations. Our benchmark can be considered as the domain-specific analogue of the general benchmark for vision tasks developed in [19, 20]. Various benchmarking frameworks for image models has been developed; in addition to VTAB, other examples include the Visual Decathlon [47]and Meta-Dataset [48], etc. While general image benchmarks are useful for evaluating the quality of general visual representations; domain-specific benchmarks better reflect the adaptability of visual representations to tasks most relevant to

cardiac ultrasound, i.e., models that perform well on general benchmarks may not necessarily be the best models to finetune for tasks involved in echocardiography.

Available backbones		Reference
Convolutional Neural Networks (CNN)	ResNet ResNeXt DenseNet Inception MobileNet ConvNext	[22] [23] [24] [25] [26] [27]
Vision Transformers (ViT)	Mix Transformer encoders (MiT) Pyramid Vision Transformer (PVT) Multi-scale vision Transformer (ResT) PoolFormer UniFormer Dual Attention Vision Transformers (DaViT)	[28] [29] [30] [31] [32] [49]

Table S2: List of all available backbones in ETAB.

Available task-specific heads				
Classification and regression heads (still image)	Standard linear probe			
Classification and regression heads (video clips)	RNN + Linear output layer LSTM + Linear output layer			
Segmentation heads	U-Net U-Net++ MAnet Linknet PSPNet DeepLabV3 SegFormer TopFormer			

Table S3: List of all task-specific heads in ETAB.

Representation		ETAB scores		
	•	•	•	•
ResNet50-ImageNet-S	0.85	0.61	0.68	0.55
ResNet50-ImageNet-SSL	0.82	0.59	0.61	0.53
ResNet50-3DSeg8-S	0.89	0.73	0.72	0.63

Table S4: Breakdown of the ETAB scores by task categories for various representations.

B Description of the benchmark task codes

Each task adaptation benchmark is encoded through an 5-character code that describes the properties of the benchmark tasks of the form XX-XX-X. The characters within each code encode the tasks as:

• Characters 0-1: Task identified

- Characters 2-3: View identifier
- Characters 4-5: Dataset identifier

The data sets are encoded as follows **E**: EchoNet, **C**: CAMUS, and **T**: TMED. The views are encoded as follows: **A2**: Apical 2-chamber, **A4**: Apical 4-chamber, **PL**: parasternal long axis, and **PS**: parasternal short axis. The 4 tasks categories are encoded as **a**, **b**, **c** and **d**. The task identifiers are defined as:

(a) Cardiac Structure Identification Tasks

- 0: Segmenting the left ventricle (LV)
- 1: Segmenting the left atrium (LA)
- 2: Segmenting the myocardial wall (MY)

(b) Cardiac Function Estimation Tasks

- 0: Estimating LV ejection fraction
- 1: Classifying end-systole and end-diastole frames

(c) View Recognition Tasks

- 0: Classifying apical 2- and 4-chamber views
- 1: Classifying parasternal short and long axis views

(d) Clinical Prediction Tasks

- 0: Diagnose cardiomyopathy
- 1: Diagnose aortic stenosis

C Experimental setup

The ETAB software library can be accessed through this link: https://github.com/ahmedmalaa/ETAB. The library provides thorough documentation and step-by-step instructions for the ETAB benchmarking framework, as well as code snapshots to reproduce our experiments. The documentation provides a description of the ETAB API which can be used to run any benchmark experiment out-of-the-box. The ETAB website also contains a continuously updated leaderboard with a list of all supported backbone representations along with their corresponding ETAB scores.

Baselines and hyper-parameters. The ETAB library currently supports 12 backbone representations. We define a backbone representation as a general-purpose frame embedding for echocardiograms that is independent of the benchmark task category, whereas the head changes based on the task. The backbone representations supported in ETAB fall into two categories: convolutional neural networks and vision transformers. The list of all backbone representations in ETAB are listed in Table S2. Links to the hyperparameter configurations and architectural specifications for all backbones are provided in the online ETAB leaderboard.

All experiments were conducted using an SGD optimizer with a batch size of 32, a learning rate of 0.001 and 50 training epochs. For each benchmark task, the corresponding echocardiogram dataset was split into a 60% training sample, 10% validation sample and a 40% testing sample.

Breakdown of the ETAB benchmark results. The ETAB protocol allows evaluating pre-trained representations both on an aggregate level or with respect to each task category. Table S4 shows the performance of different pre-trained representations with respect to the 4 task categories.